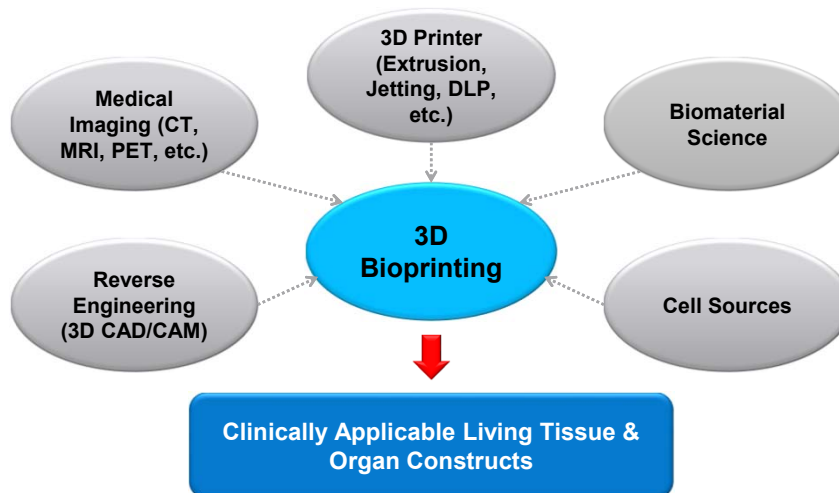


BIOINK DEVELOPMENT & PRINTABILITY FOR COMPLEX 3D PRINTING

Sang Jin Lee, Ph.D.

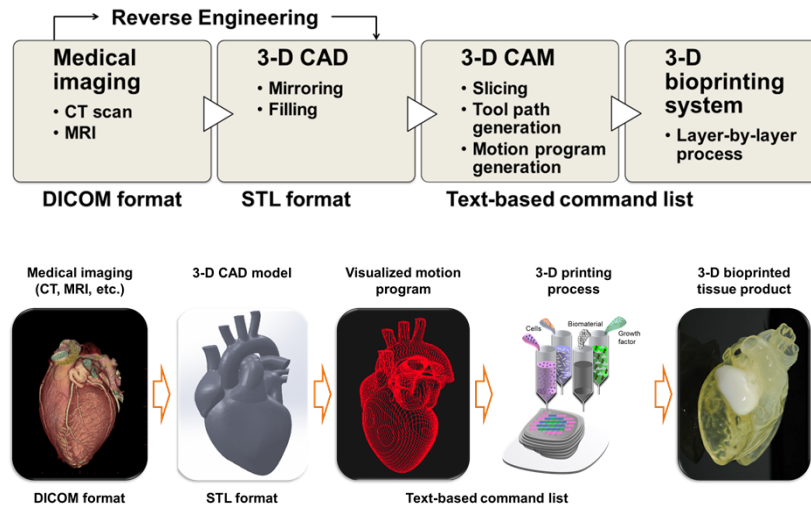
1

Definition of 3D Bioprinting



2

3D Bioprinting Workflow

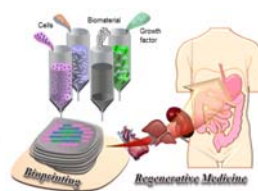


3

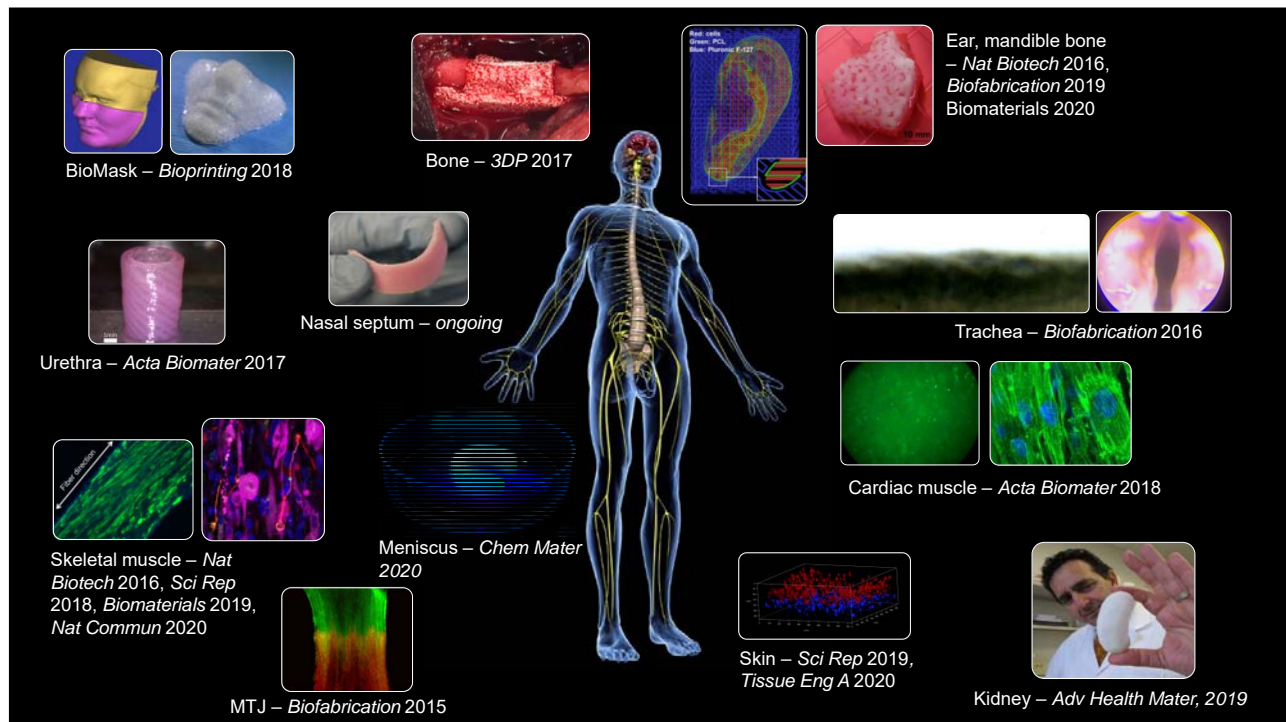
Integrated Tissue-Organ Printing (ITOP) System

ITOP can concurrently print synthetic biodegradable polymers and cell-laden hydrogels in a single tissue construct with clinically applicable size and shape with structural integrity for tissue engineering applications

- Generation of 3D freeform shaped constructs with precision
 - Multiple cell types, biomaterials, drugs
- High strength constructs:
 - Hydrogels and polymers (~12)
- Printing resolution:
 - Cell printing: $\geq 50 \mu\text{m}$
 - Structural polymer printing: $\geq 2 \mu\text{m}$



4



5

3D Bioprinting - Bioinks

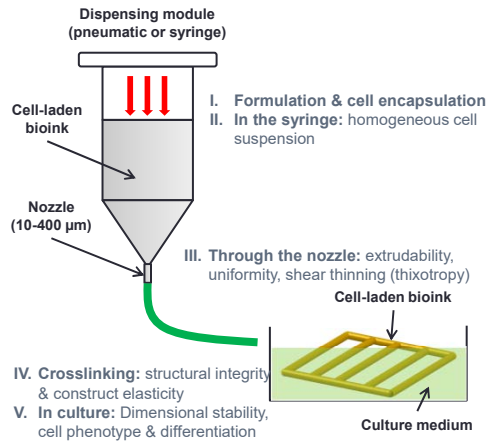
- A major challenge for tissue and organ engineering is *the production of 3D biomimetic, cellular tissue constructs* of clinically relevant size and shape with structural integrity
- 3D bioprinting can print *cell-laden hydrogels to manufacture complex, multi-cellular living tissue constructs* that mimic the structure of native tissues
- *Bioinks* provide the biological microenvironment needed for the successful delivery of cells and biomaterials to discrete locations within 3D structures
- To improve and enhance the significance and innovation of this approach, it is critical to develop *standardized bioink systems*

6

6

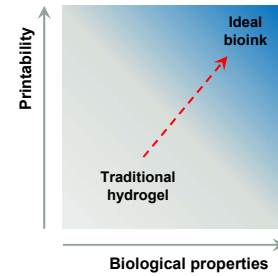
Hydrogel-based Extrusion Bioprinting

Required properties of bioinks



Working Definitions of Printability

- 1. Extrudability**
 - How difficult is it to extrude the bioink?
 - Pressure required to extrude the bioink at a given flowrate
- 2. Extrusion uniformity/accuracy**
 - Are the extrusion lines straight and uniform?
 - Length of an extrusion line's edge relative to a perfectly uniform filament
- 3. Structural integrity**
 - Does the bioink hold its shape after extrusion?
 - Height of a printed structure



Biological properties

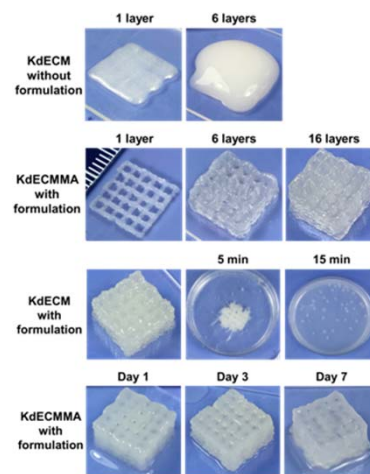
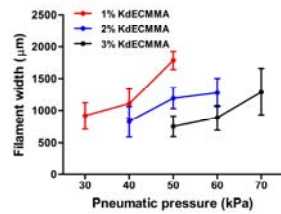
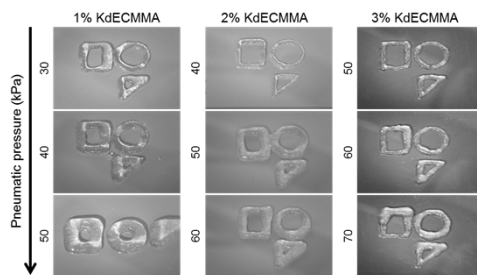
- Non-toxic
- Supporting cell growth
- Maintaining cell phenotype
- Accelerating tissue formation

7

Gillispie et al. *Biofabrication*. 2020

7

Determination of Printing Parameters



8

Ali et al., *Adv Healthcare Mater* 2019

8

Hydrogels Available for Bioprinting

Hydrogels

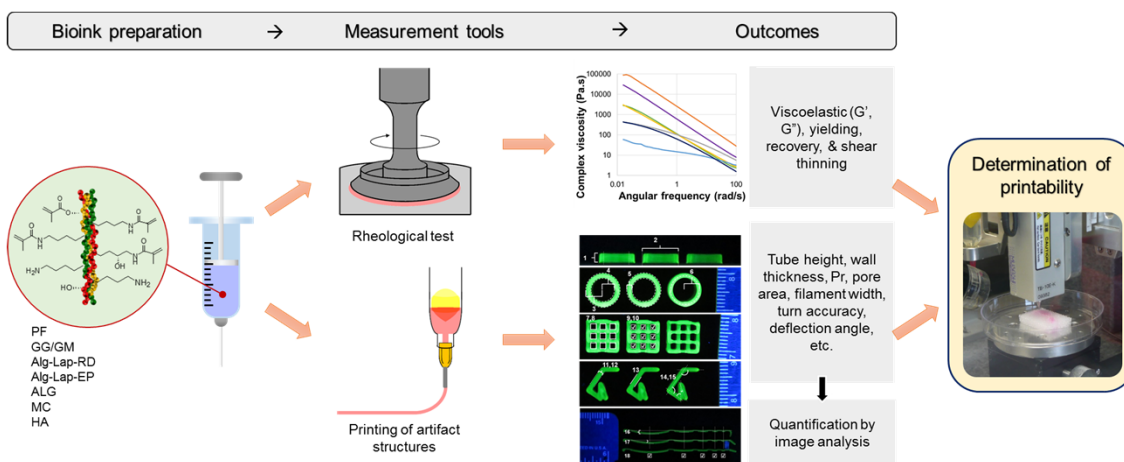
- Collagen
- Fibrinogen
- Hyaluronic acid (HA)
- Sodium alginate
- Gelatin
- Methyl cellulose
- Gellan gum
- Chitosan
- Agarose
- Xantan gum
- Poly(ethylene glycol) (PEG)
- Pluronic F127

Quantitative printability measurement is needed

- Most often, printability is described qualitatively
- Rheological measurement for the extrudability and shear-thinning property of materials
- Yet, predicting the final shape of a printed construct have been inconclusive
- The relationships between rheology and other aspects of printability are not fully understood - rheology cannot yet be used as a proxy for printability
- Direct measures of printability are currently needed in order to confirm the suitability of bioinks for specific bioprinting applications.

9

Strategy of Bioink Development

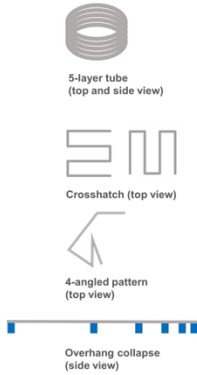


10

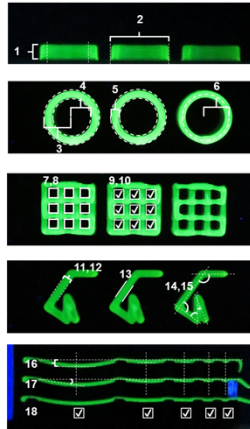
10

Bioink Artifact for Printability Measurement

Printing patterns

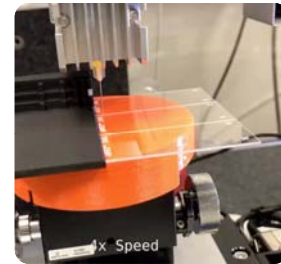


Printing outcomes



Printability measurement

Structure	View	Printability Aspect	Measures	Calculation
5-Layer Tube	Side	• Stack multiple layers	¹ Height	Direct measurement
			² Width	Direct measurement
5-Layer Tube	Top	• Stack multiple layers	³ External radius	$r_e = \sqrt{A_e/\pi}$
			⁴ Internal radius	$r_i = \sqrt{A_i/\pi}$
			⁵ Wall thickness	$T = r_e - r_i$
			⁶ Radial accuracy	$r_a = \frac{(r_e + r_i)/2}{4} \times 100\%$
Crosshatch	Top	• Form horizontal pores	⁷ P_r	$P_r = \frac{L_p^2}{16A_p}$
			⁸ Area of pores	Direct measurement
			⁹ # of broken pores	Direct measurement
4-angled pattern	Top	• Sharp turns	¹⁰ # of filled pores	Direct measurement
			¹¹ Filament width	Direct measurement
			¹² Standard deviation of filament width	$\sigma_w = \sqrt{\frac{\sum(w_i - \bar{w})^2}{N_w}}$
			¹³ Uniformity ratio	$U = \frac{(P_1 + P_2)/2}{L_f}$
			¹⁴ Turn angle	Direct measurement
Overhang Collapse	Side	• Span gaps unsupported	¹⁵ Turn angle error	$\theta_e = \theta_m - \theta_s$
			¹⁶ Deflection at midpoint	Direct measurement
			¹⁷ Angle of deflection	$\theta_d = \sin^{-1}(D/0.5G)$
			¹⁸ Spanning success rate	Direct measurement



The artifact possesses excellent ease of use, printing in **less than 10 min**, using less than **0.4 mL of bioink**, and an automated image analysis process.

Gillispie et al., under review

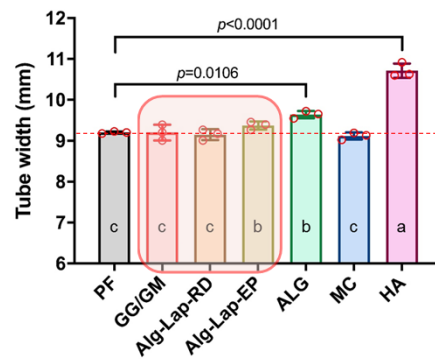
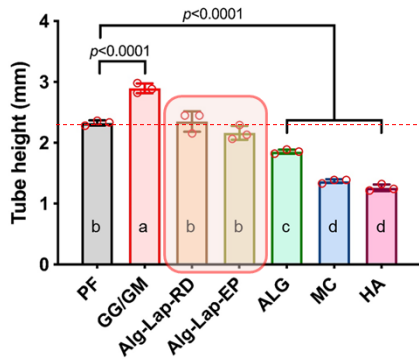
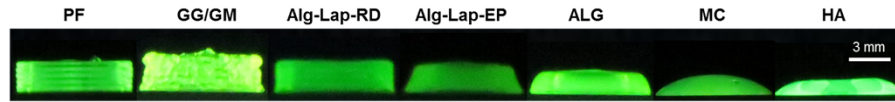


Selected Testing Bioink Formulations

Abbr.	Formulation	Selection criteria	Printing conditions				
			Pressure (kPa)	Flowrate (mm ³ /min)	Feedrate (mm/min)	Layer height (μm)	Nozzle size (μm)
PF	40% Pluronic F127	Standard bioink	258				
GG/GM	1.2% Gellan Gum + 4% GelMA	Testing formulation	164				
Alg-Lap-RD	1% Alginate + 6% Laponite RD	2nd high printability comparator	140				
Alg-Lap-EP	1% Alginate + 6% Laponite EP	Testing formulation	75	84	150	420	330
ALG	7% Alginate	Viscose hydrogel	742				
MC	8% Methylcellulose	Poor shape fidelity	602				
HA	3% Hyaluronic Acid	Poor shape fidelity	174				



5-layer Tube (Side View)



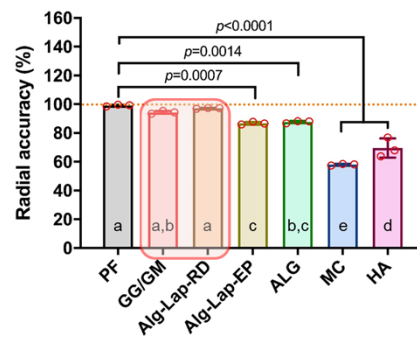
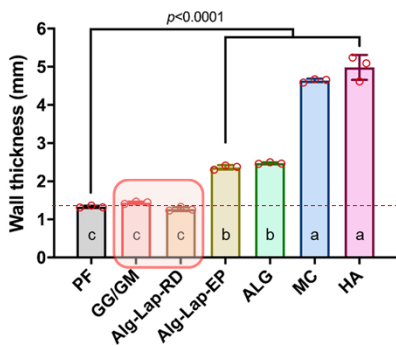
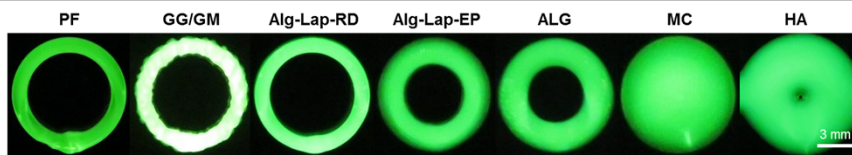
13

Gillispie et al., under review



13

5-layer Tube (Top View)



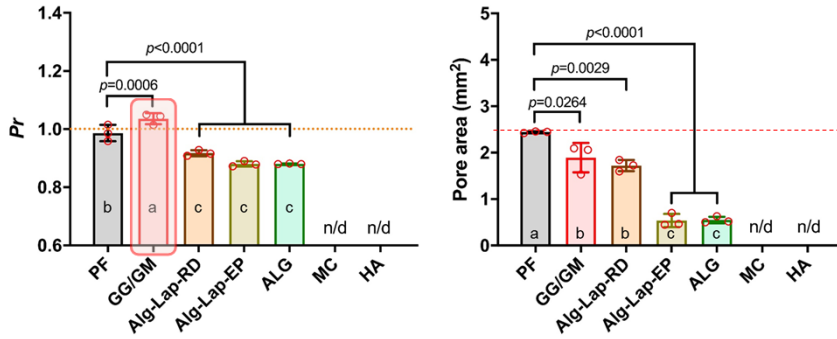
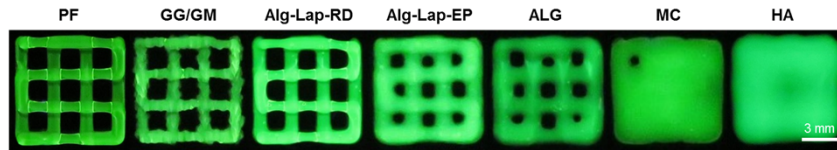
14

Gillispie et al., under review



14

Crosshatch



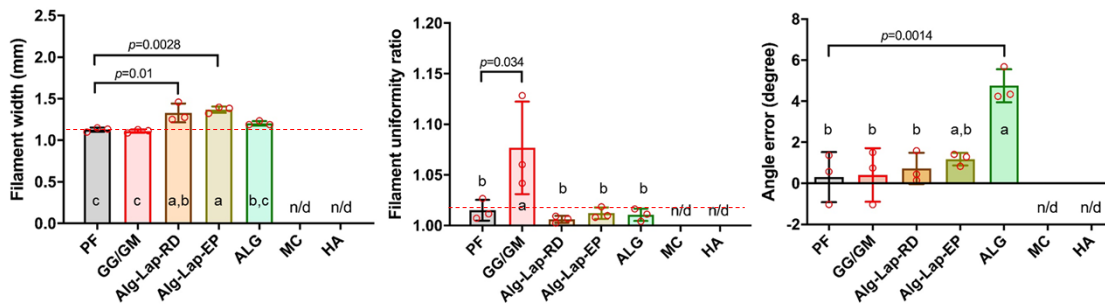
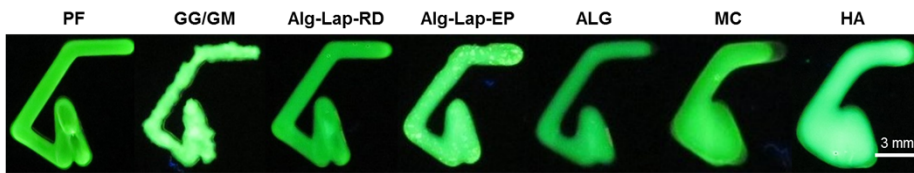
15

Gillispie et al., under review



15

4-Angled Pattern



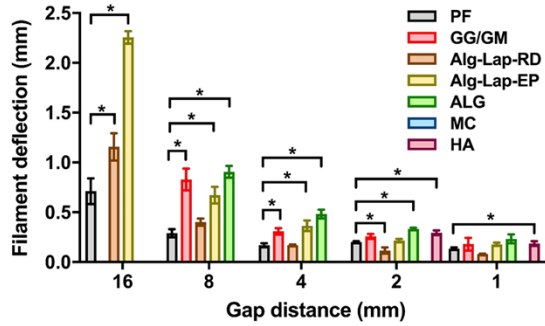
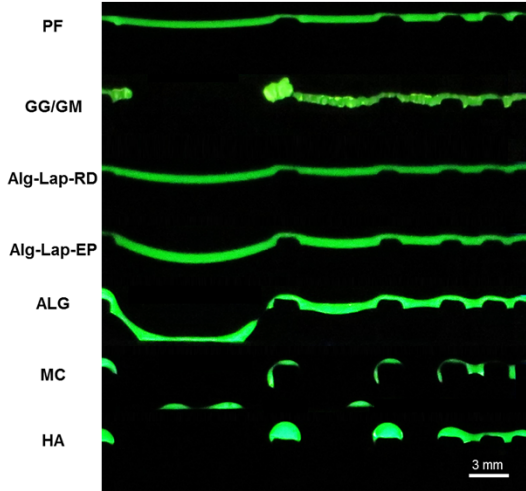
16

Gillispie et al., under review



16

Overhang Collapse



17

Gillispie et al., under review



17

Printability Outcomes

Abbr.	Printing conditions									
	Tube height	Tube width	Wall thickness	Radial accuracy	Pr	Pore area	Filament width	Uniformity	Angle error	Filament deflection
PF (standard)	+++	+++	+++	+++	+++	+++	+++	+++	+++	+++
GG/GM	++	+++	+++	+++	+++	+++	+++	+	+++	+
Alg-Lap-RD	+++	+++	+++	+++	++	++	++	+++	+++	+++
Alg-Lap-EP	+++	+++	++	++	+	+	++	+++	+++	++
ALG	+	++	++	++	+	+	+++	+++	+	+
MC	+	+	+	+	n/d	n/d	n/d	n/d	n/d	+
HA	+	+	+	+	n/d	n/d	n/d	n/d	n/d	+

+++ Good; ++ Intermediate; + Poor; n/d: not detectable

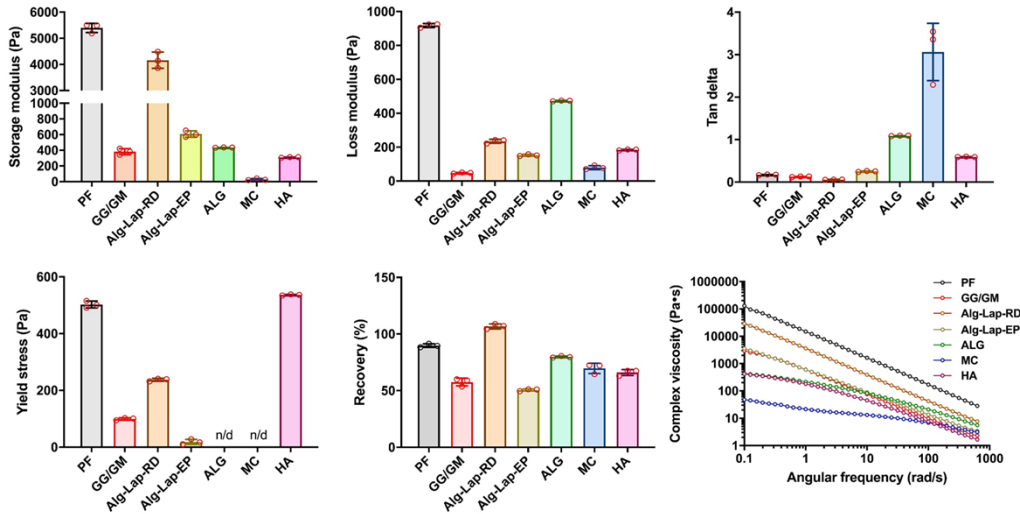
18

Gillispie et al., under review



18

Rheological Properties



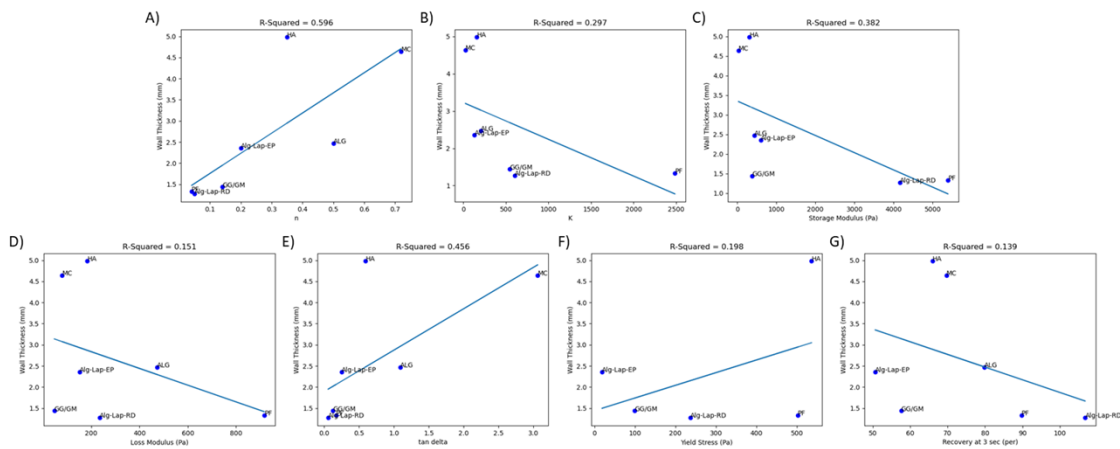
19

Gillispie et al., under review



19

Rheology vs. Printability (Linear Regression Analysis)



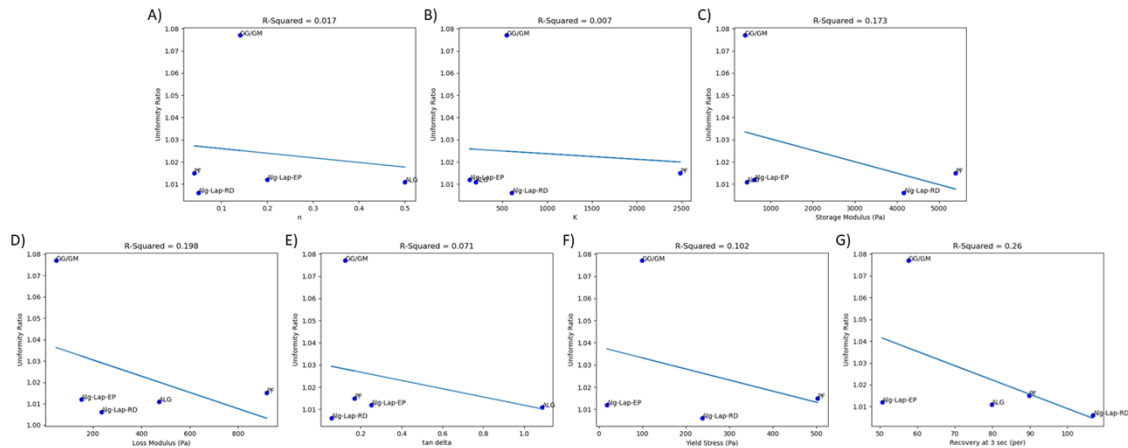
20

Gillispie et al., under review



20

Rheology vs. Printability (Linear Regression Analysis)



Gillispie et al., under review

21

21

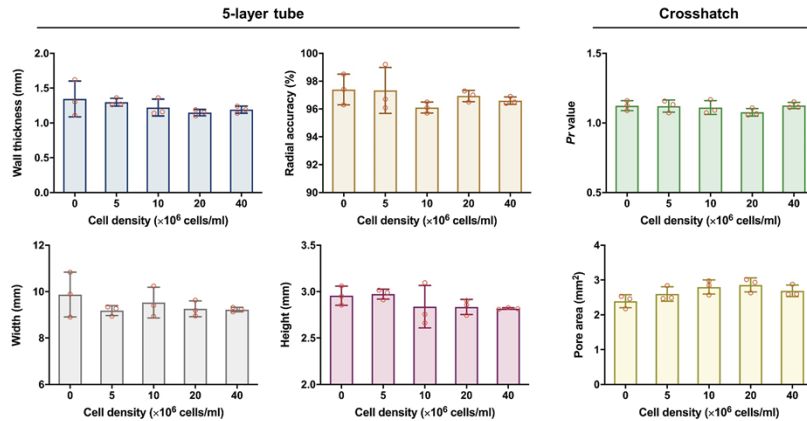
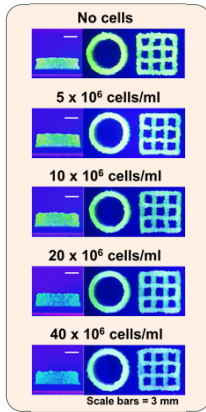
Rheological Properties vs. Printability

- Rheological measurement is valuable insight into the bioink's shear-thinning, viscoelastic, yielding, and recovery properties
- Loss modulus (G'') is not predictive of printing outcomes
- Rheological measures are not predictive of uniformity, except, low G'' may be an indicator of poor uniformity
- No rheological parameter alone was able to predict relative printability
- Printing outcomes must be measured directly rather than inferred from rheology
- Thus, standardization of printability measurement is essential for bioink development

22

22

Effect of Cell Density on Printability



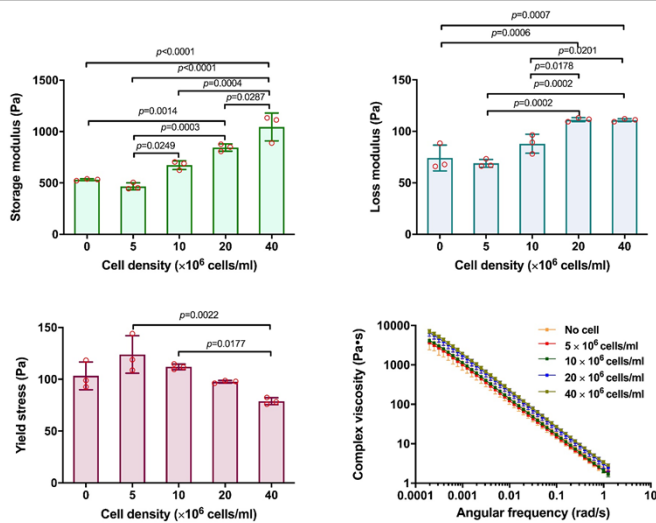
Gillispie et al., Tissue Eng 2020



23

23

Effect of Cell Density on Rheological Properties



Gillispie et al., Tissue Eng 2020



24



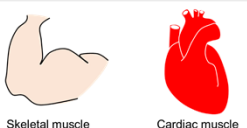
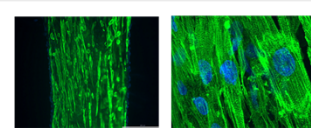
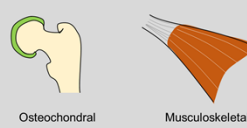
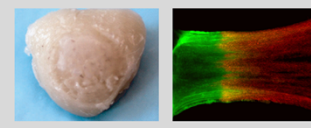
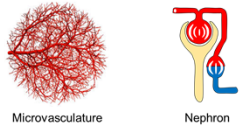
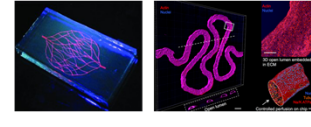
24

Effect of Cell Density on Printability

- The effect of cell density on printing outcomes have been investigated in the GelMA/GG composite bioink
- No effect on printability was seen for cell densities up to 40×10^6 cells/mL
- Rheological measures showed some variation between the bioinks with different cell densities.
- Both storage modulus (G') and loss modulus (G'') increased moderately as cell density increased
- Yield stress showed slight changes, initially increasing as cells were introduced at 5×10^6 /mL and then decreasing from there as cell density increased
- All bioinks showed similar shear-thinning abilities with analogous K and n constants

25

25

Design concept	Tissues or organs	Resolution	Applications
Shape and size	 Bone Ear Nose	< 400 μ m	
Tissue organization (alignment, etc.)	 Skeletal muscle Cardiac muscle	< 200 - 300 μ m	
Composite tissues (interface, etc.)	 Osteochondral Musculoskeletal	< 50 - 100 μ m	
Functional inner structures (vasculature, nephron, etc.)	 Microvasculature Nephron	< 10 μ m	

47

47

Acknowledgements

Faculty collaborators

- Anthony Atala, MD
- John D. Jackson, PhD
- James J. Yoo, MD, PhD

Biomaterial scientists

- Young Min Ju, PhD
- Ji Hyun Kim, PhD
- Jihoon Park, PhD

Cell biologists

- Lauren West-Livingston, PhD
- Mohamed Ali, PhD

Biomedical engineers

- Gregory J. Gillispie, PhD
- Joshua S. Copus, MS
- Hyeongjin Lee, PhD
- Juntae Huh, BS

Mechanical engineers

- Peter Prim, PhD
- Young-Wook Moon, PhD
- Eric Renteria, BS

Surgeons/physicians

- Ickhee Kim, MD, PhD
- Gabriel Galeano, MD
- Jee-Ho Lee, MD, PhD

Research technicians

- Denethia Green, MS
- Anna Young

Outside collaborators

- Hak Soo Choi, PhD, MGH
- Antonio Mikos, PhD, Rice U.
- John Fisher, PhD, Maryland
- Moon Suk Kim, PhD, Ajou U.
- Pam Yelick, PhD, Tufts U.
- Geun Hyung Kim, PhD, SKK
- Salil Desai, PhD, NC A&T
- Yong Huang, PhD, U. Florida



Supported by:



48

Thank You

Sang Jin Lee, Ph.D.

Wake Forest Institute for Regenerative Medicine

sjlee@wakehealth.edu

www.wakehealth.edu/wfirm



wfirmnews

wfirmnews

49